First Clinical Experience With the DeBakey VAD Continuous-Axial-Flow Pump for Bridge to Transplantation

Georg M. Wieselthaler, MD; Heinrich Schima, PhD; Michael Hiesmayr, MD; Richard Pacher, MD; Günther Laufer, MD; George P. Noon, MD; Michael DeBakey, MD; Ernst Wolner, MD

Background—A shortage of donor organs and increased numbers of deaths of patients on the waiting list for cardiac transplantation make mechanical circulatory support necessary for patients who die on the waiting list. Continuous-flow rotary blood pumps offer exciting new perspectives.

Methods and Results—Two male patients (ages 44 and 65 years) suffering from end-stage left heart failure were implanted with a DeBakey VAD axial-flow pump for use as a bridge to transplant. The pump is designed to achieve 5 L/min against 100 mm Hg and has a rotor speed of 10 000 rpm and a power input of 4.5±0.6 W. In both patients, the early postoperative phase was characterized by a completely nonpulsatile flow profile. However, with the recovery of heart function 8 to 12 days after implantation, increasing pulse pressures became evident, and net flow rose to 4.5±0.6 L/min, causing an increase of mean CI up to 2.7±0.2 L·min⁻¹·m⁻². Patients were mobilized and put through regular physical training. Hemolysis stayed in the physiological range and increased only slightly from 2.1±0.8 mg/dL before surgery to 3.3±1.8 mg/dL 6 weeks after implantation.

Conclusions—The first clinical implants of the DeBakey VAD axial-flow pump have demonstrated the device to be a promising measure of bridge-to-transplant mechanical support. (Circulation. 2000;101:356-359.)

Key Words: heart failure • heart-assist device • DeBakey VAD
tion and end-organ dysfunction at the time of implantation. These 2 patients were the first in our center to enroll in a multi-institutional study in Europe. The protocol for the study was approved by the Institutional Review Committee, and both patients provided written informed consent.

Operation
Like other left ventricular assist devices, this pump is implanted through a median sternotomy with extracorporeal circulation (ECC). The pump was placed in a small, left-sided extracardiac pocket. A sewing ring was attached to the apex of the beating heart with circumferentially placed buttressed sutures. An inflow cannula was inserted into the ventricle, and a Dacron skirt of the cannula was sutured to the apical ring. The Vascutec outflow graft was placed extrapericardially and anastomosed to the ascending aorta. The VAD was easily deaired, and the pump was started while ECC was gradually discontinued. A combined cardiac and pump output was maintained at a cardiac index of $2.0 \text{ L} \cdot \text{min}^{-1} \cdot \text{m}^{-2}$ obtained with a Swan-Ganz catheter.

Anticoagulation
The study protocol allowed individual anticoagulation regimens according to each center’s previous device experience. During ECC and implantation of the pump, the patient received heparin 300 U/kg body wt IV, and the heart-lung machine was primed with 1 000 000 IU aprotinin. After discontinuation of ECC, heparin was reversed with an appropriate dose of protamine. Intravenous heparin was instituted 6 hours after surgery to achieve activated partial thromboplastin target times of 50 to 60 seconds. Platelet antiaggregation therapy with 150 mg/d aspirin and 225 mg/d dipyridamole was started after removal of all chest drains. Administration of heparin was stopped when anticoagulation with coumarin reached target levels of INR 2.5 to 3.5.

Statistic Analysis
All results for continuous variables are expressed as mean±SD. Students paired or unpaired t test, if appropriate, was used to compare continuous variables between 2 subgroups. A value of $P<0.05$ was considered indicative of statistical significance.

Results
Clinical Course
The intraoperative course in both patients was uneventful, and the pump showed good performance, with flow rates of 3 to 5 L/min after gradual discontinuation of ECC, and adequate tissue perfusion was achieved with mixed venous oxygen saturation $>60\%$. However, full unloading of the extremely enlarged ventricles in this early period could not be achieved, but transesophageal echocardiography showed a closed aortic valve, and no pulsations in the aortic blood pressure curve could be detected. Pump flow increased within the first days after surgery and stabilized at flow rates of $4.5\pm 1.2$ L/min after postoperative week 3 (Figure 2). Because the aortic valve stayed closed all the time (as shown by echocardiography), we calculated a cardiac index of $2.7\pm 0.2$ $\text{L} \cdot \text{min}^{-1} \cdot \text{m}^{-2}$. After initial early extubation, both patients needed surgical reinterventions on postoperative days 5 and 6, respectively. Anticoagulation overtreatment caused bleeding in patient 1; patient 2 presented a laceration of the subclavian vein caused by catheter insertion. Subsequently, both patients were mobilized, and inotropic support for sufficient right heart function could be discontinued. Both patients were moved from the intensive care unit to an intermediate care ward and were put through regular physical training to rebuild the muscle mass lost during prolonged periods of preoperative immobilization.

Hemodynamic Changes
The initial period after implantation of the DeBakey VAD was characterized by complete nonpulsatile arterial blood pressure in both patients. Despite the aortic valve staying

<table>
<thead>
<tr>
<th>TABLE 1. DeBakey VAD Patient Demographics</th>
<th>Patient 1</th>
<th>Patient 2</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age, y/sex</td>
<td>44/M</td>
<td>65/M</td>
</tr>
<tr>
<td>Disease</td>
<td>Dilated cardiomyopathy</td>
<td>Ischemic cardiomyopathy</td>
</tr>
<tr>
<td>Intra-aortic balloon pump</td>
<td>No</td>
<td>No</td>
</tr>
<tr>
<td>Ventilation</td>
<td>No</td>
<td>No</td>
</tr>
<tr>
<td>NYHA class</td>
<td>IV</td>
<td>IV</td>
</tr>
<tr>
<td>Aortic pressure, mm Hg</td>
<td>88/54/68</td>
<td>105/54/78</td>
</tr>
<tr>
<td>Pulmonary artery pressure, mm Hg</td>
<td>69/38/48</td>
<td>48/25/32</td>
</tr>
<tr>
<td>Pulmonary capillary wedge pressure, mm Hg</td>
<td>28</td>
<td>20</td>
</tr>
<tr>
<td>Cardiac index, $\text{L} \cdot \text{min}^{-1} \cdot \text{m}^{-2}$</td>
<td>1.8</td>
<td>1.9</td>
</tr>
<tr>
<td>Pulmonary vascular resistance, dyn $\cdot$ s/cm$^2$</td>
<td>514</td>
<td>166</td>
</tr>
<tr>
<td>Intravenous medication</td>
<td>Dobutamine $5 \mu\text{g} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$</td>
<td>Dopamine $6 \mu\text{g} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$</td>
</tr>
<tr>
<td></td>
<td>Prostaglandin E $5 \text{ng} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$</td>
<td>Milrinone $0.5 \mu\text{g} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$</td>
</tr>
</tbody>
</table>
closed, modulation of pulsatility with low amplitude to the
nonpulsatile blood flow produced by the VAD could be
achieved by varying pump flow. Mean arterial blood pres-
sures were always kept in the range of 70 to 90 mm Hg, and
flow rate was adjusted to obtain mixed venous oxygen
saturation >60%. After this initial nonpulsatile period, low-
amplitude pulsations became more frequent and were asso-
ciated with recovered left ventricular contractility, but at all
times nonpulsatile flow patterns could be produced with an
increase in pump speed.

Device Performance
In both patients, the DeBakey VAD provided adequate flow
to maintain sufficient tissue perfusion expressed by mixed
venous oxygen saturation >60% in the early perioperative
period. Pump speed was set between 9000 and 11 000 rpm
and was adjusted manually in this early phase to avoid excess
suction with ventricular collapse, which was easily detected
in the pump flow curve. With hemodynamic stabilization of
the patients, pump flow increased gradually from 3.9±0.5
L/min in postoperative week 1 up to 4.5±0.6 L/min after
postoperative week 3, with peak flows >6 L/min. Sudden
pump desynchronizations followed by automatic restarts
could be detected in both patients but did not dramatically
affect patients in their daily routine. On postoperative day 60,
1 patient encountered an 18-minute, probably connector-
related pump stop, which occurred during his daily exercise
on the bicycle. The patient tolerated a regurgitation of 1.3
L/min through the pump, although he needed short-term
intravenous inotropic support. He recovered immediately
when the pump was successfully restarted and provided flows
of >5 L/min.

Hemolysis
Table 2 shows indices of hemolysis for both patients before
surgery and at 1, 2, 3, 4, 5, and 6 weeks after implantation. No
statistically significant elevation of mean plasma-free hemog
lin was detected. Serum creatinine levels declined from a
slightly elevated preoperative level to normal. Lactate dehy-
drogenase increased significantly during the postoperative
period, but only patient 2 developed peak levels of >800 U/L
4 weeks after implantation, together with elevated levels of
γ-glutamyl transferase and no correlation with single peaks in
plasma-free hemoglobin.

Discussion
Pulsatile blood pressure profile was always considered nec-
essary to maintain sufficient tissue perfusion in mammals.
Early studies with nonpulsatile blood flow in calves perfo-
ried by Johnston et al5 in 1976 gave the first evidence of

![Figure 2. Pump flow, pump speed, and pump motor current for DeBakey VAD axial-flow pump in patient 1.](http://circ.ahajournals.org/)
tolerance of this nonphysiological blood flow pattern. Later, Golding et al. were able to sustain survival for up to 34 days. Yada and associates supported calves with nonpulsatile blood flows for >3 months but hypothesized a need for an ≈20% higher blood flow than with pulsatile perfusion to avoid transient physiological disorders. In our patients, we could demonstrate for the first time that continuous blood flow, generated by an implanted axial-flow pump, over a period of >60 days is well tolerated in humans. The pumps generated low hemolysis, within physiological ranges. In accordance with the early animal experiments, these first clinical implants provide no evidence of disadvantages of this unphysiological continuous-flow condition in humans. This generates optimism for a more widespread use of implantable rotary blood pumps as long-term mechanical support. In contrast to the electric pusher-plate pumps, axial-flow pumps are silent, are smaller in size, have lower energy requirements, and provide the prospect of low device costs. Nevertheless, a number of questions are as yet unanswered. Some of them are general concerns applicable to all kinds of rotary blood pumps, such as the absence of an inherent Frank-Starling mechanism and its consequences during exercise, as well as the definition of control parameters to optimize pump-speed adjustments and avoid excess suction. Such questions as noninvasive measurement of nonpulsatile or low-pulsatile blood pressures of fully mobilized and exercising patients will have to be addressed in the future. Furthermore, episodes of stalling and consecutive pump stops and restarts have not yet been sufficiently explained. Other questions involve construction specifications of the pump, such as the geometry and diameter of the pump inflow cannulas.

In conclusion, the first clinical implants of the DeBakey VAD axial-flow pump have demonstrated the feasibility of continuous-blood-flow pumps as a promising measure of bridge-to-transplant mechanical support. This new technology opens exciting possibilities with evident advantages, but a number of questions remain open with regard to use of the pumps in humans.

Acknowledgment

The DeBakey VAD devices were provided according to an Ethics Committee–approved study protocol by MicroMed Technology Inc.

References

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